PCT

WORLD INTELLECTUAL PROPERTY ORGANIZATION International Bureau



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 7:		(11) International Publication Number:	WO 00/16697
A61B 10/00	A2	(43) International Publication Date:	30 March 2000 (30.03.00)
 (21) International Application Number: PCT/US (22) International Filing Date: 17 September 1999 ((30) Priority Data: 09/159,467 23 September 1998 (23.09.9 (71) Applicant: SENORX, INC. [US/US]; Suite 144, 136 Parkway, Irvine, CA 92618 (US). (72) Inventors: BURBANK, Fred, H.; 30982 Steeplecha San Juan Capistrano, CA 92675 (US). LUBOCK, Bethany, Laguna Niguel, CA 92677 (US). JONES, L.; 34441 Camino El Molino, Capistrano Beach, (US). QUICK, Richard, L.; 32181 Fall River Road Canyon, CA 92679 (US). (74) Agents: KLEIN, Howard, J. et al.; Klein & Szeke Suite 700, 4199 Campus Drive, Irvine, CA 92612 	(17.09.9 98) U 677 Altrase Driv , Paul; , Micha CA 926 I, Trabu	AZ, BA, BB, BG, BR, BY, CA (Utility model), DE, DE (Utility model), DM, EE, EE (Utility model), GB, GD, GE, GH, G JP, KE, KG, KP, KR, KZ, LC MD, MG, MK, MN, MW, MX SD, SE, SG, SI, SK, SK (Util TT, UA, UG, UZ, VN, YU, Z GM, KE, LS, MW, SD, SL, patent (AM, AZ, BY, KG, KZ, patent (AT, BE, CH, CY, DE IE, IT, LU, MC, NL, PT, SE, CG, CI, CM, GA, GN, GW, M Published Without international search r upon receipt of that report.	A, CH, CN, CR, CU, CZ, CZ ity model), DK, DK (Utility model), ES, FI, FI (Utility M, HR, HU, ID, IL, IN, IS, LK, LR, LS, LT, LU, LV, K, NO, NZ, PL, PT, RO, RU, ity model), SL, TJ, TM, TR, ZA, ZW, ARIPO patent (GH, SZ, TZ, UG, ZW), Eurasian MD, RU, TJ, TM), European D, DK, ES, FI, FR, GB, GR, O, OAPI patent (BF, BJ, CF, ML, MR, NE, SN, TD, TG).

(54) Title: ELECTROSURGICAL BIOPSY DEVICE AND METHOD

(57) Abstract

An electrosurgical biopsy device includes a stylet and a cannula movably mounted on a base. The stylet has a shaft with a head at its distal end and a stylet ablation element extending distally from the head. The stylet shaft is disposed through the cannula for axial translation therein between withdrawn and extended positions. The cannula has an opening at its distal end and a cannula ablation element adjacent the opening. Both ablation elements are activatable with energy that ablates adjacent tissue. A translation mechanism controllably moves (a) the stylet between the withdrawn and extended positions and (b) the cannula between a proximal position and a distal position relative to the base. In use, with the stylet in the withdrawn position against the distal end of the cannula, and with the stylet ablation element activated, the stylet and the cannula are pushed through the skin and the underlying tissue until the stylet head is adjacent a targeted tissue mass. Next, the stylet is extended distally from the distal end of the cannula so that its head penetrates the tissue mass. The cannula ablation element is then activated, and the cannula is pushed through the tissue mass toward the stylet head, thereby cutting a "core" through the tissue mass that is captured as a tissue specimen within the distal end of the cannula. The cannula and the stylet are then removed from the patient's body.

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
ΑU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
ВВ	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav	TM	Turkmenistan
BF	Burkina Faso	GR	Greece		Republic of Macedonia	TR	Turkey
BG	Bulgaria	HU	Hungary	ML	Mali	TT	Trinidad and Tobago
BJ	Benin	Œ	Ireland	MN	Mongolia	UA	Ukraine
BR	Brazil	[L	Israel	MR	Mauritania	UG	Uganda
BY	Belarus	IS	Iceland	MW	Malawi	US	United States of America
CA	Canada	IT	Italy	MX	Mexico	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NE	Niger	VN	Viet Nam
CG	Congo	KE	Kenya	NL	Netherlands .	YU	Yugoslavia
СН	Switzerland	KG	Kyrgyzstan	NO	Norway	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's	NZ	New Zealand		
СМ	Cameroon		Republic of Korea	PL	Poland		
CN	China	KR	Republic of Korea	PT	Portugal		
cυ	Cuba	KZ	Kazakstan	RO	Romania		
cz	Czech Republic	LC	Saint Lucia	RU	Russian Federation		
DE	Germany	LI	Liechtenstein	SD	Sudan		
DK	Denmark	LK	Sri Lanka	SE	Sweden		
EE	Estonia	LR	Liberia	SG	Singapore		
j							

WO 00/16697

1	ELECTROSURGICAL BIOPSY DEVICE AND METHOD
2	
3	CROSS-REFERENCE TO RELATED APPLICATIONS
4	Not Applicable
5	
6	FEDERALLY SPONSORED RESEARCH OR DEVELOPMENT
7	Not Applicable
8	
9	BACKGROUND OF THE INVENTION
10	The present invention relates to devices and methods for removing a
11	sample of tissue from a human or animal. In particular, the present invention
12	pertains to devices and methods for conducting a biopsy to remove a sample or
13	specimen of a tumor or lesion for examination and analysis.
14	In diagnosing and treating certain medical conditions, such as
15	potentially cancerous tumors, it may be desirable to extract from a portion of
16	suspicious tissue, such as a tumor, a specimen of the suspicious tissue for
17	detailed examination and analysis. The process of removing such a specimen
18	of tissue is referred to as a biopsy.
19	In many instances, the suspicious tissue to be examined is inside the
20	patient's body. For example, the suspicious tissue may be a tumor inside a
21	human breast. To minimize surgical intrusion into the body, it is desirable to
22	be able to insert a small instrument into the body for extracting a portion of the
23	suspicious tissue.
24	Different types of instruments and procedures have been developed for
25	conducting biopsies to extract a tissue specimen for analysis. One device that
26	has been developed is the fine needle aspirator. This device comprises a
27	hollow needle, the end of which is sharpened. The needle is inserted into the
28	suspicious tissue so that individual cells or clusters of cells of the tissue lodge

WO 00/16697

28

1 inside the hollow core of the needle. The needle is then extracted from the 2 patient, and the cells and fluid removed from the needle for a cytological 3 examination. In certain circumstances, however, it may be desirable to extract 4 portions of tissue for a histological examination, a procedure that is not 5 typically feasible using a fine needle aspirator. 6 Another type of tissue-sampling device for biopsies is exemplified by 7 the device described in U.S. Patent No. Re.34,056 - Lindgren et al. This type 8 of device includes a forward stylet, which includes at its distal end a sharpened 9 cutting surface. The stylet may be, for example, a needle sized between 12 and 20 gauge. Behind the sharpened cutting end of the stylet, along the shaft 10 11 thereof, is a groove. A hollow cannula surrounds the stylet, and has its distal 12 end sharpened to form a fine cutting edge. A mechanism is provided to move 13 the stylet and the cannula forward separately. For example, springs may be 14 used for this purpose. Preferably, the stylet and the cannula are moved 15 forward rapidly so that the sharpened ends thereof may efficiently cut the 16 tissue. In operation, the operator of this type of device first causes the stylet to 17 be pushed forward through the tumor or suspect tissue. After the distal end of 18 the stylet has passed through the suspect tissue, a portion of the tissue 19 surrounding the stylet partially fills the groove on the shaft of the stylet. The cannula is then pushed forward so that the sharpened distal end of the cannula 20 21 cuts off the portion of the tissue that has filled the groove on the shaft of the 22 stylet, and encloses that tissue. The entire device may then be removed from 23 the patient's body, and the tissue trapped in the cannula removed for 24 examination and analysis. 25 U.S. Patent No. 5,526,822 - Burbank et al. discloses another type of 26 biopsy device that includes the ability to apply a vacuum to the groove in the 27 stylet. This vacuum assists in drawing tissue into the groove, ensuring that a

more substantial portion of tissue is severed by the cutting cannula. Using

1	such a system, it is in some cases possible to use a relatively large stylet (e.g.,
2	a 7 to 14 gauge needle) to obtain a relatively large tissue sample.
3	All of the above-described systems use knife edges to a cut the tissue.
4	The cutting edge must remain extremely sharp, so that it cuts the tissue
5	cleanly. Moreover, the stylet and the cannula cutter must be propelled forward
6	rapidly to provide a clean cut through the tissue. Elaborate mechanisms are
7	typically employed to provide the rapid forward movement. Because the
8	knife edges move rapidly, however, there is limited time for tissue to fill the
9	groove on the stylet. Therefore, the system sometimes obtains a smaller
10	sample than would be ideal. In addition, variations in tissue density and
11	anatomy may cause the stylet to deflect from its ideal position in relation to the
12	tissue to be penetrated.
13	Electrosurgical techniques have been used in a variety of
14	circumstances, including certain types of biopsies. In electrosurgery, high
15	frequency electrical energy is applied through a primary electrode to tissue.
16	The electrical energy flows through the tissue to a return electrode. The tissue
17	adjacent to the primary electrode is ablated, to form an opening in the tissue.
18	The return electrode in monopolar electrosurgery may be a large electrode
19	placed on the exterior of the patient's body at a point remote from the primary
20	electrode. In bipolar electrosurgery, the return electrode may be a smaller
21	electrode positioned somewhat near the primary electrode. An exemplary
22	biopsy instrument using electrosurgical techniques is described in International
23	Publication No. WO 98/08441.
24	
25	SUMMARY OF THE INVENTION
26	The present invention, in one aspect, is a novel electrosurgical tissue
27	sampling device, or biopsy device, including a novel electrosurgical stylet. In
28	another aspect, the present invention is a method of using the novel biopsy

WO 00/16697

1

2

3

4

5

6

7

8

9

10

11

12

13

14

15

16

17

18

19

20

21

22

23

24

25

26

27

28

device to obtain a tissue specimen.

The novel stylet of the present invention includes a shaft that has a proximal end and a distal end. At the distal end of the stylet shaft is a substantially hemispherical head. A stylet electrode extends distally from the stylet head. The stylet electrode may be activated with radio frequency (RF) electrical energy to ablate the tissue adjacent the stylet electrode. A cannula that cooperates with the stylet also has a proximal end and a distal end. An opening is formed at the distal end of the cannula. The distal end of the cannula may be selectively separated from the stylet, or may abut the stylet to close the opening at the distal end of the cannula. Also at the distal end of the cannula is another electrode that also may be activated with radio-frequency electrical energy to ablate the tissue adjacent the distal end of the cannula. The system may be monopolar, in which the return electrical path is provided by a return electrode attached to the patient's body remote from the device. Alternatively, the system may be bipolar, in which the return electrical path is provided by a return electrode on the device itself. The same return electrical path may be used for both the electrode on the stylet and the electrode on the cannula. In accordance with the method of the present invention, the electrode on the head of the stylet is energized. With the stylet in a withdrawn position abutting against the distal end of the cannula, the stylet and the cannula are pushed through the skin and the underlying tissue, while applying an RF current, until the head of the stylet is adjacent a targeted tissue mass (e.g., a lesion or tumor). Next, the stylet is extended distally from the distal end of the

head and the distal end of the cannula are on opposite sides of the tissue mass.

The electrode at the distal end of the cannula is then energized, and the cannula is pushed through the tissue mass toward the stylet head, thereby

cannula so that its head penetrates the targeted tissue mass, whereby the stylet

1	cutting a "core" through the tissue mass that is captured as a tissue specimen
2	within the distal end of the cannula. The cannula and the stylet are then
3	removed from the patient's body. After the cannula and the stylet have been
4	removed, they may be separated from one another, and the tissue specimen
5	enclosed within the cannula may be removed and examined.
6	
7	BRIEF DESCRIPTION OF THE DRAWINGS
8	Figure 1 is a perspective view of a preferred embodiment of a biopsy
9	device constructed in accordance with the present invention;
10	Figure 1A is a perspective view of a portion of the cannula and stylet of
11	a modified form of the preferred embodiment of the biopsy device;
12	Figure 2 is a distal end view of the device illustrated in Figure 1, taken
13	from the left side of Figure 1;
14	Figure 3 is a perspective view, partially broken away, of a preferred
15	embodiment of an electrosurgical stylet constructed in accordance with an
16	aspect of the present invention, and incorporated in the device illustrated in
17	Figure 1;
18	Figure 4 is a top view of the device of Figure 1, with the device set to
19	begin a biopsy procedure in accordance with the method of the present
20	invention;
21	Figure 5 is a second top view, similar to the view of Figure 4, of the
22	device of Figure 1, with the stylet extended for an intermediate step of a
23	biopsy procedure in accordance with the method of the present invention;
24	Figure 6 is a third top view, similar to the view of Figure 4, of the
25	device of Figure 1, with both the stylet and the cannula extended for a further
26	stage of a biopsy procedure in accordance with the method of the present
27	invention;
28	Figure 7 is a cross-sectional view taken along line 7-7 of Figure 6;

1	Figure 8 is a cross-sectional view taken along line 8 - 8 of Figure 6;
2	Figure 9 is a staggered cross-sectional view taken along line 9 - 9 of
3	Figure 4;
4	Figure 10 is a cross-sectional view taken along line 10 - 10 of Figure 9;
5	Figure 11 is a cross-sectional view taken along line 11 - 11 of Figure
6	10;
7	Figure 12 is a cross-sectional view of the cannula and stylet, taken
8	along line 12 - 12 of Figure 6;
9	Figure 13 is a view taken along line 13 13 of Figure 5, showing a
10	distal end view of the cannula, and a cross-sectional view of the stylet shaft;
11	Figure 14 is a cross-sectional view taken along line
12	14 - 14 of Figure 12;
13	Figure 15 is a cross-sectional view of the base of the biopsy device,
14	taken along line 15 - 15 of Figure 7;
15	Figure 16 is a side elevational view of an alternative embodiment of the
16	electrosurgical stylet that may be incorporated in the biopsy device of the
17	present invention;
18	Figure 17 is a perspective view of an alternative embodiment of the
19	cannula portion of the biopsy device of the present invention;
20	Figure 18 illustrates the step of inserting the biopsy device into tissue
21	for extracting a tissue specimen, in accordance with the method of the present
22	invention;
23	Figure 19 illustrates the biopsy device positioned to begin extracting a
24	tissue specimen in accordance with the method of the present invention;
25	Figure 20 illustrates the biopsy device at an intermediate step of the
26	biopsy procedure in accordance with the method of the present invention; and
27	Figure 21 illustrates the biopsy device at a later intermediate step of the
28	biopsy procedure in accordance with the method of the present invention.

1 2

DETAILED DESCRIPTION OF THE INVENTION

Referring first to Figure 1, a particular preferred embodiment of a biopsy device 100, constructed in accordance with the present invention, is illustrated. The biopsy device 100 includes a probe 102, a base unit 104, an energy source, such as a radio-frequency generator 106, and a control unit 108.

The probe 102 includes a stylet 110 and a cannula 112. The stylet 110 electrosurgically separates tissue through the use of an electrical current activated at high frequency, such as a frequency in the radio frequency range. The stylet 110, when electrically activated, ablates tissue adjacent its electrically active components.

The stylet 110, comprising an aspect of the present invention, is shown in Figure 3. The stylet 110 includes a stylet head 122 having a substantially cylindrical body with a substantially hemispherical surface at the distal end of the stylet head 122. The stylet head 122 is formed of an electrically insulating material, such as a plastic. The stylet head 122 is attached to the distal end of a stylet shaft 124, which is also formed of an electrically insulating material. The stylet shaft 124 may have a central longitudinal bore through it, preferably along the longitudinal axis of the shaft 124.

A conductive metal stylet electrode 126 protrudes distally from the stylet head 122. In the illustrated embodiment, the stylet electrode 126 is formed of an arcuate length of electrical conductor that protrudes from diametrically opposite sides of the stylet head 122, and extends over the hemispherical distal end surface of the stylet head 122. The radius of curvature for the stylet electrode 126 is substantially coplanar with the longitudinal axis of the stylet shaft 124. The stylet electrode 126 forms a first tissue ablation element for electrosurgically separating tissue so as to create an

1 incision.

2 For the purposes of the present description of the invention, the term "ablation", as used in this specification, is defined as the process of creating an 3 incision by vaporizing tissue. The preferred embodiment described herein 4 uses electrical energy in the radio frequency range for the ablation process. 5 6 However, tissue ablation may also be accomplished with other energy sources, such as microwaves or ultrasound. In such cases, the configuration of the 7 8 ablation elements may differ from the ablation electrodes described 9 hereinbelow. The energy supply and control system may differ as well. The 10 appropriate variations and modifications in these components to accommodate 11 the alternative energy sources will suggest themselves to those skilled in the pertinent arts. 12 13 The stylet electrode 126 merges into a single stylet electrical conductor 14 128 inside the stylet head 122. The single stylet electrical conductor 128 15 extends through the central bore in the stylet shaft 124. The stylet conductor 16 128 is electrically connected with both ends of the stylet electrode 126. 17 An alternative embodiment of the stylet head is illustrated in Figure 16. 18 The embodiment illustrated in Figure 16 includes a conical head 130 that has 19 an electrically conductive apex portion 132 that forms the stylet electrode. 20 The apex portion is secured to the distal end of an insulative, frustrum-shaped 21 base portion 134. The conical stylet electrode 132, which forms the stylet 22 tissue ablation element, is in electrical contact with the stylet conductor 128 23 (as described above with reference to Figure 3). 24 The cannula 112 is formed of an elongated hollow outer tube 140 25 (Figures 12, 13, and 14) that has a distal end and a proximal end. Preferably, 26 the longitudinal axis of the cannula 112 coincides with the longitudinal axis of the stylet shaft 124. The outer tube 140 of the cannula 112 is formed of an 27 28 electrically nonconductive or insulating material, such as plastic, and may be

formed by extrusion. For example, the outer tube 140 of the cannula may be 1 2 formed of a polyimide. The outer surface of the cannula tube 140 may be 3 coated with TEFLON® (polytetrafluoroethylene) or similar low-friction polymeric material to reduce sticking between the surface and the surrounding 4 5 tissue. 6 At the distal end of the cannula 112 is a cannula electrode 142 forming 7 a second tissue ablation element. The cannula electrode 142 may be formed of the distal end of a tubular conductor 144 extending along the length of the 8 9 cannula 112, inside the outer tube 140. 10 An electrically insulating inner sleeve 146 may cover the inner surface of the tubular conductor 144. The inner cannula sleeve 146 may also be 11 formed by extrusion of a polyimide. The inner surface of the inner cannula 12 13 sleeve 146 may be coated with a low-friction polymeric material, such as 14 TEFLON®. The inner insulating sleeve 146 is spaced from the stylet shaft 124 to form an annular passage 148 that is open at the distal end of the cannula 15 16 112. The annular passage 148 receives tissue samples that are severed by the 17 cannula electrode 142, as described below. 18 In a bipolar configuration for the probe, described below, the cannula 19 112 will include other elements 152, 156, shown in Figures 12, 13, and 14. 20 These other elements, described below, are not incorporated in the monopolar 21 configuration. 22 The stylet 110 and the cannula 112 may be moved relative one another 23 along their common longitudinal axis. For example, the stylet 110 may be 24 moved relative to the cannula 112 between an extended position in which the distal end of the stylet shaft 124 and the stylet head 122 are separated from the 25 distal end of the cannula 112, and a withdrawn position in which the stylet 26

head 122 abuts or is in close proximity to the distal end of the cannula 112.

Those familiar with electrosurgical techniques will understand that

27

PCT/US99/21416

when a high frequency electrical current is applied to a primary electrode, such

2 as the stylet electrode 126, and the primary electrode is exposed to tissue, the

3 tissue adjacent the primary electrode is ablated. To perform such

4 electrosurgery, a return electrical path through the tissue is required, to close

5 the electrical circuit.

WO 00/16697

An electrosurgical device may be either monopolar or bipolar. With a monopolar device, the return electrical path is provided through a return electrode that may be a grounded contact pad that is applied to the exterior of the patient's body at a point remote from where the primary electrode is placed in the body. With a bipolar device, the return electrical path is provided from the primary or ablation electrode through a return electrode that is located relatively near the primary electrode. The bipolar return electrode is contained on the same instrument body as the primary electrode. Although parts of the present invention are described with reference to a monopolar configuration, and parts are described with reference to a bipolar configuration, those skilled in the art will recognize how the device may be implemented in either configuration.

In the monopolar configuration of the biopsy device illustrated in Figure 1, a patient return pad 150 is attached to the patient's body, and is in electrical contact with the RF generator 106. The patient return pad 150 forms a return electrode for the energy delivered by the RF generator 106 to the stylet electrode 126 and the cannula electrode 142. In the monopolar configuration, the annular conductor 144 that terminates in the cannula electrode 142 is disposed between the external insulating layer of the tube 140, and the inner insulating sleeve 146.

A probe 102' used in the bipolar configuration of the biopsy device in accordance with the present invention is shown in Figure 1A. In the bipolar configuration, the return electrical path is provided through a conductor

1 contained within a bipolar cannula 112'. Referring to Figures 12, 13, 14, and 1A, the additional elements of the bipolar cannula 112' are shown. A 2 3 conductive layer 152 is contained just under the outer tube 140, and forms a return path electrode. A pair of diametrically-opposed longitudinal side 4 openings or slots 154 (one of which is shown in Figure 1A) are provided in the 5 6 outer tube 140. These side openings 154 may extend longitudinally along a 7 substantial portion of the length of the cannula 112'. Through these openings 8 154 in the outer tube 140, the conductive layer 152 forming the return path 9 electrode is exposed to the environment surrounding the cannula 112'. Thus, when the probe 102' (Figure 1A) is inserted into a patient's tissue, the return 10 11 electrode 140 is in contact with the tissue, and electrical current may flow through the tissue from the stylet electrode 126 and the cannula electrode 142 12 13 to the return electrode 152. The return electrode is advantageously 14 electrically connected to ground potential. Referring now particularly to Figure 12, the annular cannula conductor 15 16 144 in a bipolar implementation is spaced from the return path electrode 152 17 by an insulating layer 156 of non-conductive material, such as plastic. The 18 insulating layer 156 electrically isolates the return path electrode 152 from the 19 cannula conductor 144. 20 When activated with a current oscillating at high frequency (such as in 21 the radio frequency range), the cannula electrode 142 ablates tissue adjacent to 22 the cannula electrode. As with the stylet electrode 126, the operation may be 23 either monopolar or bipolar. For operation in accordance with a bipolar 24 technique, the same return electrode 152 used with the stylet electrode 126 may also be used in conjunction with the cannula electrode 142. However, 25 those skilled in the art, taking the teaching provided herein, will also recognize 26 27 that alternative electrical return paths may be provided.

An alternative embodiment of the cannula is illustrated in Figure 17.

12

1 This particular alternative embodiment is illustrated as a monopolar device. 2 However, those skilled in the art will recognize that the illustrated embodiment 3 may be modified to add a return electrode to implement a bipolar embodiment. In the alternative embodiment illustrated in Figure 17, the cannula is formed of 4 5 a cannula body 160. A cannula conduit 162 extends along the length of the 6 cannula body 160. A length of conductor extends through the cannula conduit 7 162, and is formed into a substantially circular cannula electrode 164 that coincides with the distal end of the cannula body 160. Those skilled in the art 8 9 will readily recognize that other configurations may be used to form the cannula electrode at the distal end of the cannula. For example, the cannula 10 conduit 162 may be formed as a groove cut along the length of the cannula 11 12 body 160. Similarly, the cannula conduit 162 may be formed on the interior 13 surface of the cannula body 160. 14 An energy source, such as the radio-frequency generator 106, generates the electrical current required for application to the stylet electrode 126 and the 15 cannula electrode 142. The design, construction, and operation of such a 16 17 generator and control unit are conventional and well-understood by those 18 familiar with electrosurgery technology. 19 The base unit 104 controls the position and movement of the stylet 110, 20 the cannula 112, and the application of the electrical energy generated by the 21 generator and control unit 106 to the stylet electrode 126 and the cannula 22 electrode 142. The base unit 104 permits the cannula 112 and stylet 110 to be 23 moved together, and also to be moved separately. For example, the probe 102, including both the stylet 110 and the cannula 112, may be moved between an 24 extended position relative to the base unit 104 in which the distal end of the 25 stylet 110 and the distal end of the cannula 112 are relatively farther from the 26 27 base unit 104, and a withdrawn position in which the distal end of the stylet

110 and the distal end of the cannula 112 are relatively closer to the base unit

13

1 104. Furthermore, the base unit 104 may extend the stylet 110 between an 2 extended position relative to the cannula 112, and a withdrawn position 3 relative to the cannula 112. 4 The base unit 104 may be enclosed in a housing 202 (shown in 5 phantom lines in Figure 1). The housing 202 protects the internal elements of 6 the device. The housing 202 may be substantially sealed to protect the internal 7 elements of the base unit 104 from contamination during use of the stylet 110 8 and cannula 112 during a biopsy procedure. However, the housing 202 may 9 be selectively removable, or have an access panel (not shown) provided to 10 allow access to certain elements within the base unit 104. In addition, the 11 housing 202 may be shaped to facilitate hand holding of the device, or it may 12 be configured to be attached to other devices (not shown) for holding the 13 biopsy device in the proper position for conducting the biopsy procedure. 14 Referring now to Figures 1, 4, 5, and 6, the base unit 104 includes a 15 base 204 to which is fixed an electric motor 206 (preferably a DC motor 16 powered by a power supply 207). The motor 206 is employed for moving the 17 stylet 110 and the cannula 112 relative to the base unit 104. A cannula carrier 18 210 is slidably mounted on the base 204. The cannula 112 has a proximal end 19 that is attached to a cannula carrier 210. The cannula carrier 210 translates the 20 cannula 112 longitudinally on the base unit 104. The stylet shaft 124 has a 21 proximal end that is attached to a stylet carrier 220 that is slidably mounted on 22 the base 204. The stylet carrier 220 translates the stylet 110 longitudinally on 23 the base 204. In combination with the cannula carrier 210, the stylet carrier 24 220 also translates the stylet 110 relative to the cannula 112. The motor 206 includes a drive shaft 221 to which is attached a drive screw 222. The drive 25 26 screw 222 is threaded through a screw-driven slide 224 that moves the cannula 27 carrier 210 and the stylet carrier 220 in the manner described below. 28 The stylet 110 and the cannula 112 are preferably separable from the

14

stylet carrier 220 and the cannula carrier 210, respectively. In this way, the

- 2 entire probe unit 102, including the stylet 110 and cannula 112, may be
- 3 replaced upon each use, without having to replace the entire device. This
- 4 allows the stylet 110 and cannula 112 to be disposable, so that a new, sterile
- 5 stylet and cannula may be used for each biopsy procedure.

The proximal end of the stylet 110 may be embedded in or attached to a

- 7 stylet foot 225, formed of an electrically insulating material, such as plastic.
- 8 The stylet foot 225 is removably mounted in the stylet carrier 220. For
- 9 example, the stylet foot 225 may fit into a correspondingly shaped recess in
- 10 the stylet carrier 220. A stylet retention strip 227, having its two ends
- 11 removably attached to the stylet carrier 220, and extending across the top of
- the stylet foot 225, retains the stylet foot 225 in the stylet carrier 220.

Similarly, the proximal end of the cannula 112 may be embedded in or

attached to a cannula foot 229, formed of an electrically insulating material,

15 such as plastic. The cannula foot 229 is removably mounted in the cannula

carrier 210, such as by being retained in a correspondingly shaped recess in the

cannula carrier 210. A cannula retention strip 231, having its two ends

18 removably attached to the cannula carrier 210, and extending across the

cannula foot 229, retains the cannula foot 229 in the cannula carrier 210.

The entire probe unit 102, including the stylet 110 and the cannula 112

21 may be made available to medical doctors and hospitals as a single modular

22 unit, ready for attachment to the base unit 104. In this way, the sterility of the

23 probe unit 102 may be maintained. After completion of a biopsy procedure,

24 the entire probe unit 102 may then be removed from the base unit 104 and

25 discarded in accordance with proper procedures for medical waste.

28

An exemplary mounting for the cannula carrier 210 on the base 204 is

27 illustrated in Figure 7. The base 204 includes substantially U-shaped channels

226 along each side thereof. Horizontal extensions 228 of the bottom portion

1 of the cannula carrier 210 engage these channels 226. The mounting of the 2 cannula carrier 210 on the base 204 preferably provides very little friction 3 between the cannula carrier 210 and the base 204. A low friction mounting 4 helps to ensure smooth and accurate movement of the cannula carrier 210 5 relative to the base 204. 6 The mounting of the stylet carrier 220 on the base 204 is 7 advantageously similar to the mounting of the cannula carrier 210. An 8 exemplary mounting for the stylet carrier 220 on the base 204 is illustrated in 9 Figure 8. Horizontal extensions 230 of the bottom portion of the stylet carrier 220 engage the U-shaped channels 226 formed in the base 204. The mounting 10 11 of the stylet carrier 220 on the base 204 preferably provides very little friction 12 between the stylet carrier 220 and the base 204. A low friction mounting helps 13 to ensure smooth and accurate movement of the stylet carrier 220 relative to 14 the base 204. 15 The base 204 includes a plurality of stops that define the maximum 16 extent of the longitudinal movements of the cannula carrier 210 and the stylet carrier 220 along the base 204. In the particular embodiment illustrated, an 17 18 end piece 232 is provided at the distal end of the base 204. The end piece 232 19 forms a forward stop for the cannula carrier 210. An intermediate stop 234 is 20 affixed to the base 204. The distal side of the intermediate stop 234 forms a 21 rearward stop for the cannula carrier 210, while the proximal side of the 22 intermediate stop 234 forms a forward stop for the stylet carrier 220. A back 23 stop 236 is affixed to the base 204 as a rearward stop for the stylet carrier 220. 24 The cannula carrier 210 may be moved between a withdrawn position (illustrated in Figures 4 and 5) and an extended position (illustrated in Figure 25 26 6). In the withdrawn position, the distal edge of the cannula carrier 210 is spaced from the end piece 232 of the base 204, and the proximal edge of the 27

cannula carrier 210 abuts against the distal side of the intermediate stop 234.

In this withdrawn position, the cannula 112 is withdrawn relative to the base 1 2 204. When the cannula carrier 210 is in the extended position, the distal edge 3 of the cannula carrier 210 abuts against the end piece 232, and the cannula 112 4 is extended distally with respect to the base 204. As the cannula carrier 210 moves toward the distal end of the base 204, the cannula 112 moves distally 5 6 with respect to the base 204. As the cannula carrier 210 moves toward the 7 proximal end of the base 204, the cannula 112 moves proximally with respect 8 to the base 204. 9 The stylet carrier 220 may also be moved between a withdrawn position (illustrated in Figure 4) and an extended position (illustrated in Figures 5 and 10 11 6). In the withdrawn position, the distal edge of the stylet carrier 220 is spaced 12 from the intermediate stop 234, and the proximal edge of the stylet carrier 220 13 abuts against the back stop 236. In this withdrawn position, the stylet 110 is withdrawn relative to the base 204. When the stylet carrier 220 is in the 14 15 extended position, the distal edge of the stylet carrier 220 abuts against the 16 proximal side of the intermediate stop 234. As the stylet carrier 220 moves 17 longitudinally on the base 204 toward the distal end of the base, the stylet 110 18 moves distally with respect to the base 204. As the stylet carrier 220 moves 19 longitudinally on the base 204 toward the proximal end of the base, the stylet 20 110 moves proximally with respect to the base 204. 21 A drive mechanism on the base 204 moves the cannula carrier 210 and 22 the stylet carrier 220. In the particular embodiment illustrated, the drive 23 mechanism includes the electric motor 206, the drive screw 222, and the 24 screw-driven slide 224. The screw-driven slide 224 is slidably mounted on the 25 base 204 so as to be movable between a proximal position in which it is 26 relatively near the motor 206, and a distal position in which the it is relatively 27 remote from the motor 206, and nearer the distal end of the base 204. The

movement of the screw-driven slide 224 controls the movement of the cannula

1 carrier 210 and the stylet carrier 220.

2 The screw-driven slide 224 is moved along the base 204 by the drive screw 222, which in turn is driven by the motor 206 by means of the drive 3 4 shaft 221. The motor 206 rotates the drive shaft 221 and the screw 222, the 5 latter engaging threads (not shown) in the screw-driven slide 224 to move the 6 screw-driven slide 224 along the base 204. When the motor 206 rotates in a 7 first direction (for example, clockwise), the motor turns the drive screw 222 in 8 the same direction, which in turn moves the screw-driven slide 224 from its 9 proximal position toward its distal position. When the motor 206 rotates in the opposite direction, the rotation of the screw 222 moves the screw-driven slide 10 11 224 in the opposite direction, toward its proximal position. 12 A pair of push rods 240 are fixed to the distal side of the screw-driven 13 slide 224. Each of these push rods 240 extends through openings (not shown) 14 in the stylet carrier 220, so that the distal ends of the push rods 240 may 15 engage the proximal side of the cannula carrier 210. A spring bias is provided 16 between the screw-driven slide 224 and the stylet carrier 220. This spring bias 17 tends to maintain a specific predetermined separation between the screw-18 driven slide 224 and the stylet carrier 220. This spring bias may be provided by a pair of coil springs 242, each of which surrounds one of the push rods 19 20 240. 21 The mechanical operation of the base unit 104 will now be described 22 with reference to Figures 4, 5, and 6. Referring first to Figure 4, the biopsy 23 device is illustrated in a configuration in which it is set to begin a biopsy 24 procedure. The stylet 110 is withdrawn relative to the cannula 112 so that the 25 stylet 124 abuts against the distal end of the cannula 112. The cannula 112 26 and stylet 110 are both withdrawn to the full extent possible relative to the 27 base 204; that is, they are at their respective proximal limits of travel relative to the base 204.

1 As the motor 206 is operated, it turns the screw 222, which moves the 2 screw-driven slide 224 toward the distal end of the base 204 in the manner 3 described above. The springs 242 between the screw-driven slide 224 and the 4 stylet carrier 220 maintain the predetermined spacing between the screw-5 driven slide 224 and the stylet carrier 220, thus causing the stylet carrier 220 to 6 move toward the distal end of the base 204 at approximately the same rate as 7 the screw-driven slide 224. However, the cannula carrier 210 remains in its 8 original position. Thus, the stylet 110 extends distally relative to the cannula 9 112, so that the stylet head 122 separates from the distal end of the cannula 10 112. This continues until the distal ends of the push rods 240 contact the 11 proximal side of the cannula carrier 210, as illustrated in Figure 5. At this 12 stage, the stylet head 122 is spaced from the distal end of the cannula 112, 13 forming a gap between the proximal end of the stylet head 122 and the distal 14 end of the cannula 112. 15 Also at this stage, the distal side of the stylet carrier 220 contacts the 16 proximal side of the intermediate stop 234, blocking further movement of 17 these stylet carrier 220 toward the distal end of the base 204. As the motor 206 continues to rotate the drive screw 222, it continues to move the screw-18 19 driven slide 224 toward the distal end of the base 204. However, further 20 movement of the stylet carrier 220 is blocked. As the spring bias provided by the springs 242 is overcome, the springs 242 compress, and the screw-driven 21 22 slide 224 moves closer to the stylet carrier 220. As the screw-driven slide 224 23 moves closer to the stylet carrier 220, the push rods 240 extend from the distal 24 side of the stylet carrier 220 and engage the proximal side of the cannula 25 carrier 210. As the screw-driven slide 224 continues to move toward the distal end of the base 204, the push rods 240 move the cannula carrier 210 toward 26 the distal end of the base 204. This forward (distal) movement of the cannula 27 carrier 210 moves the cannula 112 relative to the stylet 110, closing the gap 28

19

between the stylet head 122 and the distal end of the cannula 112, so that the 1 2 stylet 110 is withdrawn relative to the cannula 112. 3 When the distal end of the cannula 112 contacts the proximal end of 4 stylet head 122 (as illustrated in Figure 6), further forward (distal) movement 5 of the cannula carrier 210 should be stopped. Forward movement of the cannula carrier 210 toward the distal end of the base 204 may be stopped by 6 7 stopping the motor 206. The components of the device, including the base 204 8 and the stops 232, 234, 236, may also be dimensioned so that at that point the 9 distal side of the cannula carrier 210 contacts the end piece 232 of the base to 10 stop further movement of the cannula carrier 210 in the distal (forward) 11 direction. 12 As noted previously, the energy for the stylet electrode 126 and the cannula electrode 142 is supplied by the RF generator 106. Furthermore, the 13 control of activation of the electrodes 126, 142, as well as control of the motor 14 15 206 that moves the cannular carrier 210 and the stylet carrier 220, is provided by the control unit 108. Accordingly, electrical paths must be provided to 16 17 conduct energizing current through the base unit 104 from the RF generator 106 to the stylet electrode 126 and the cannula electrode 142, and to conduct 18 control signals from the control unit 108 to the motor 206. (Control signals 19 20 are also sent from the control unit 108 to the RF generator 106 to control the 21 activation of the electrodes 126, 142.) In addition, a return electrical path must be provided for the patient return pad 150 (monopolar configuration) or the 22 23 return electrode 152 (bipolar configuration). 24 Referring now to Figure 15, the base 204 includes a plurality of electrical connectors 260a, 260b, 260c, 260d for providing electrical 25 connection to the RF generator 106 and the control unit 108, and to the power 26 supply 207 for the motor 206. A stylet lead 262, a cannula lead 264, and (in a 27

bipolar configuration only) a return lead 266 each have a first end that is

WO 00/16697

20

PCT/US99/21416

internally connected to separate ones of the connectors 260a-d. The other end 1 2 of the stylet lead 262 is connected to a stylet base contact 268 that is fixed with 3 respect to the base 204. For example, the stylet base contact 268 may be embedded in the intermediate stop 234. Similarly, the other end of the cannula 4 5 lead 264 is connected to a cannula base contact 270 that is fixed with respect 6 to the base 204. For example, the cannula lead contact 264 may be embedded 7 in the base end piece 232. 8 The return lead 266 is included only in the bipolar configuration. It is 9 not necessary in the monopolar configuration that includes the remote patient 10 return pad 150 (Figure 1). In the monopolar configuration, the connection 11 between the patient return pad 150 and the RF generator and control unit 106 12 may be provided externally to the base unit 104. The return lead 266 in the 13 bipolar configuration may be connected to a cannula return base contact 272 14 that is fixed with respect to the base 204. For example, the return base contact 15 272 may also be embedded in the base end piece 232. 16 Referring next to Figure 9, the structure of the proximal ends of the stylet 110 and the cannula 112, and the electrical paths for the stylet conductor 17 128 and for the cannula conductor 144, are illustrated. Referring first to the 18 electrical path for the stylet 110, the stylet base contact 268 is provided in the 19 intermediate stop 234. A stylet wire 274 provides an electrical current path 20 21 between the stylet base contact 268 and a stylet carrier contact 276 on the 22 stylet carrier 220. Because the position of the stylet carrier 220 changes with respect to the intermediate stop 234, the stylet wire 274 should be able to 23 accommodate changes in the physical separation between the stylet carrier 220 24 and the intermediate stop 234 while maintaining a connection between the 25 stylet base contact 268 and the stylet carrier contact 276. For example, the 26 stylet wire 274 may be a coiled wire wrapped around a longitudinal pin 278. 27 An opening 279 may be provided in the distal side of the stylet carrier 220 to 28

21

1 accommodate the coiled stylet wire 274.

2 The stylet carrier contact 276 remains in contact with an extension 3 portion 280 of a stylet carrier terminal 282 that is mounted in the stylet foot 225. The stylet carrier terminal 282, in turn, is in electrical contact with the 4 5 stylet electrical conductor 128 (see Figures 12 and 13) that is enclosed in the stylet shaft 124. The stylet carrier terminal extension portion 280 may be 6 7 formed as a spring to help maintain contact between the stylet carrier terminal 8 extension portion 280 and the stylet carrier contact 276. The stylet carrier 9 terminal 282 (with the extension portion 280) is fixed within the stylet foot 10 225, so that when the stylet foot 225 is removed from the stylet carrier 220, the 11 stylet carrier terminal 282 (with the extension portion 280) is removed with the 12 stylet foot 225. The extension portion 280 fits through an opening in the stylet 13 carrier 220 so that the extension portion may contact the stylet carrier contact 14 276. A similar type of electrical path is provided for the cannula conductor 15 142 that is contained in the cannula 112. A cannula carrier terminal 286 is 16 17 fixed within the cannula foot 229, which is removably mounted in the cannula 18 carrier 210, as previously described. The cannula carrier terminal 286 is in 19 electrical contact with the cannula conductor 144 that is enclosed within the 20 cannula tube 140. (See also Figure 10.) The cannula carrier terminal 286 has a spring extension portion 288 that is in contact with a cannula carrier contact 21 22 290 when the cannula foot 229 is mounted in the cannula carrier 210. A cannula wire 292 provides an electrical current path between the cannula 23 carrier contact 290 with the cannula base contact 270 that is embedded in the 24 base end piece 232. Again, because the position of the cannula slide 210 25 26 changes with respect to the base end piece 232, the cannula wire 292 is advantageously a coiled wire wrapped around a longitudinal pin 294. 27

A series of electrical contacts and electrical wires substantially similar

to those for providing the electrical current path for the cannula conductor 144 2 may be provided in the bipolar configuration in which a return electrode 152 is 3 included in the cannula 112. For example, the return electrical path may be 4 included on the opposite side of the cannula carrier 220 for providing contact 5 between the cannula return electrode 152 and the return base contact 272 that is embedded in the base end piece 232. A return electrode 298 embedded in 6 7 the electrically insulating cannula foot 229 (Figures 10 and 11) provides a 8 portion of such electrical contact. A coiled return wire 302 (Figures 4 and 5) 9 provides an electrical current path between the return electrode 298 and the 10 return base contact 272 embedded in the base end piece 232. The coiled return 11 wire 302 may be wrapped around a supporting longitudinal pin 304. 12 A method of performing a biopsy in accordance with an aspect of the 13 present invention will be described with reference to Figures 18 through 21. Referring first to Figure 18, a portion of human tissue, such as a human breast 14 15 410, is illustrated containing several tissue masses 420, which may be 16 suspected tumors or lesions to be examined. Through an incision in the tissue 17 410, the portion of the biopsy probe 102 containing the stylet 110 and the 18 distal end of the cannula 112 is inserted, using RF current, until the stylet head 19 122 is near a targeted tissue mass 420. The probe 102 is guided toward the 20 targeted tissue mass 420 using conventional imaging techniques, such as 21 ultrasound or X-rays. The stylet 110 and the cannula 112 are both in their 22 withdrawn (proximal) positions, as illustrated in Figure 4. Insertion of the 23 probe 102 toward the targeted tissue mass 420 may be assisted by energizing 24 the stylet electrode 126 to ablate subcutaneous tissue between the skin and the targeted tissue mass 420. As shown in Figure 19, while the probe 102 is being 25 26 inserted to access the targeted tissue mass 420, the stylet 110 is in its 27 withdrawn position relative to the distal end of the cannula 112, so that stylet 28 head 122 abuts or substantially abuts the distal end of the cannula 112, closing

the opening in the distal end of the cannula 112, and thus the passage 148. 1 2 The stylet electrode 126 is then electrically activated to ablate the tissue 3 of the targeted tissue mass 420. The stylet head 122 is then pushed through 4 the tissue mass 420, creating an opening through the tissue mass 420 as the stylet 110 penetrates the tissue mass by moving distally toward its extended 5 6 position, while the cannula 112 remains in its proximal position, so that the 7 stylet head 122 separates from the distal end of the cannula 112. A gap is thus 8 opened between the stylet head 122 and the distal end of the cannula 112. A 9 portion of the tissue mass 420 fills in this gap between the stylet head 122 and 10 the cannula 112, around the stylet shaft 124. A particular advantage of the arcuate stylet electrode 126 is that it creates a narrow "slice" through the 11 12 targeted tissue mass 420, thereby facilitating the filling of the aforesaid gap 13 with the portions of the tissue mass on either side of the "slice" that collapse 14 into the gap after being pushed outwardly by the passage of the stylet head 122. 15 16 The stylet electrode 126 may then be deactivated, and the cannula electrode 142 activated. With the cannula electrode 142 activated, the portion 17 18 of the tissue mass 420 adjacent the cannula electrode 142, is ablated, and the 19 cannula 112 may be pushed forward through the portion of the tissue mass 420 20 that has filled in around the stylet shaft 124. As the cannula 112 moves 21 through the tissue mass 420, it cuts off a portion of the tissue mass 420, and 22 encases that portion in the annular channel 148 within the cannula 112. Once the cannula 112 has closed the gap between the distal end of the cannula 112 23 24 and the stylet head 122, the severed portion of the tissue mass 420 is contained 25 within the annular channel 148 of the cannula 112. The entire probe 102 may 26 then be removed from the tissue mass 420 and the patient's body. Once removed, the cannula 112 and the stylet 110 may again be separated, and the 27 28 tumor portion contained within the annular channel 148 of the cannula 112

PCT/US99/21416 WO 00/16697

24

removed for examination and analysis. 1

28

2 Using the device and method of the present invention, the removal of 3 tissue specimens may proceed at a slower pace than is typically possible using 4 conventional spring-activated knife cutters. In particular, additional time can be allowed between the insertion of the stylet through the suspicious tissue, 5 6 and the insertion of the annular cannula. This additional time allows more of 7 the tissue to fill the space surrounding the stylet shaft 124, allowing the 8 cannula electrode 142 to cut a larger sample of the suspicious tissue than has 9 typically been possible using the cutters of the prior art. In addition, the stylet 10 and cannula of the present invention are less likely to be deflected as they 11 move through the tissue then are the mechanical cutters of prior art biopsy 12 devices. 13 The specific embodiments described and illustrated above are 14 exemplary, and not exhaustive or exclusive. Those familiar with the art will recognize that various modifications may be made to the specific embodiments 15 16 described above without departing from the concepts of the present invention. 17 For example, those skilled in the art will recognize that various modifications 18 may be made to the base unit, and that different configurations may be used 19 for controlling the movement and position of the stylet and the cannula. In 20 addition, different specific shapes of the stylet, the stylet head, and cannula 21 may be incorporated into a system implementing the present invention. Furthermore, although an electric motor is the preferred mechanism for 22 23 driving the cannula carrier and the stylet carrier, other mechanisms, such as 24 mechanical springs or pneumatic mechanisms, may be employed. Indeed, a simplified device may employ manually-driven carriers. Moreover, although 25 RF energy is preferred to effect the tissue ablation, other types of energy (e.g., 26 microwave, ultrasound, or laser) may be employed instead, as mentioned 27 above. These and other modifications and variations that may suggest

- themselves are considered to be within the spirit and scope of the present
- 2 invention, as defined in the claims that follow.

1	WHAT IS CLAIMED IS:
2	1. An electrosurgical stylet, comprising:
3	a shaft having a proximal end and a distal end and defining a
4	longitudinal axis therebetween;
5	a head fixed to the distal end of the shaft; and
6	a tissue ablation electrode extending distally from the head.
7	
8	2. The electrosurgical stylet of Claim 1, wherein the head has a
9	substantially hemispherical distal surface, and wherein the tissue ablation
10	electrode comprises an arcuate length of electrical conductor having a radius
11	of curvature that is substantially coplanar with the longitudinal axis of the
12	shaft.
13	
14	3. The electrosurgical stylet of Claim 1, wherein the head is
15	substantially frustoconical having an apex portion, and wherein the electrode
16	includes the apex portion.
17	
18	4. A biopsy device, comprising:
19	an elongate cannula tube having a distal and a proximal end;
20	a first tissue ablation element on the distal end of the cannula;
21	an elongate stylet disposed within the cannula for axial
22	translation therein between an extended position and a withdrawn
23	position and having a distal end; and
24	a second tissue ablation element on the distal end of the stylet.
25	
26	
27	5. The biopsy device of Claim 4, wherein the stylet comprises:
28	a shaft having a proximal end and a distal end and defining a

- WO 00/16697

PCT/US99/21416

^	7
Z.	1

1	longitudinal axis therebetween; and
2	a substantially hemispherical head fixed to the distal end of the
3	shaft, the second tissue ablation element extending distally from the
4	head.
5	
6	6. The biopsy device of Claim 5, wherein the first and second ablation
7	elements are activated by radio frequency electrical current, and wherein the
8	second ablation element comprises an arcuate length of electrical conductor
9	having a radius of curvature that is substantially coplanar with the longitudinal
10	axis of the shaft.
11	
12	7. The biopsy device of Claim 4, wherein the stylet comprises:
13	a shaft having a proximal end and a distal end and defining a
14	longitudinal axis therebetween; and
15	a conical head terminating in an apex portion, wherein the
16	second tissue ablation element includes the apex portion.
17	
18	8. The biopsy device of Claim 4, wherein the first and second tissue
19	ablation elements are activatable by an energy source so as to effect tissue
20	ablation.
21	
22	9. The biopsy device of Claim 8, wherein the energy source is a radio
23	frequency energy source.
24	
25	10. The biopsy device of Claim 4, further comprising stylet translation
26	means connected to the stylet for translating the stylet within the cannula
27	between the withdrawn and extended positions.
28	

- WO 00/16697

1	11. The biopsy device of Claim 10, wherein the device includes a base,
2	wherein the stylet has a proximal end extending proximally from the proximal
3	end of the cannula, and wherein the translation means comprises:
4	a carrier connected to the proximal end of the stylet and movably
5	mounted on the base, the carrier being movable on the base between a
6	first position in which the stylet is in the withdrawn position and a
7	second position in which the stylet is in the extended position; and
8	carrier drive means, coupled to the carrier, for moving the carrier
9	between the first and second positions.
10	
11	12. The biopsy device of Claim 11, wherein the carrier drive means is
12	driven by a motor.
13	
14	13. The biopsy device of Claim 12, wherein the motor has a drive
15	shaft, and wherein the carrier drive means comprises:
16	a drive screw coupled for rotation with the drive shaft;
17	a screw-driven mechanism coupled between the drive screw and
18	the carrier, whereby rotation of the drive screw in a first direction
19	moves the carrier from the first position to the second position.
20	
21	14. A biopsy device, comprising:
22	a base having a proximal end and a distal end;
23	an elongate cannula having an open distal end and an open
24	proximal end mounted on the base for axial translation thereon between
25	a proximal position and a distal position;
26	an elongate stylet disposed substantially coaxially within the
27	cannula, the stylet having a proximal end that extends proximally from
28	the proximal end of the cannula and that is mounted on the base for

I	axial translation between a withdrawn position and an extended
2	position with respect to the cannula, the stylet having a distal end;
3	a first tissue ablation element on the distal end of the cannula;
4	a second tissue ablation element on the distal end of the stylet;
5	and
6	translation means for sequentially moving the stylet from its
7	withdrawn position to its extended position, and then moving the
8	cannula from its proximal position to its distal position.
9	,
10	15. The biopsy device of Claim 14, wherein the translation means
11	comprises:
12	a first carrier, connected to the proximal end of the stylet and
13	slidably mounted on the base for translation thereon between a first
14	position corresponding to the withdrawn position of the stylet and a
15	second position corresponding to the extended position of the stylet;
16	a second carrier, connected to the proximal end of the cannula
17	and slidably mounted on the base between the first carrier and the distal
18	end of the base, for translation thereon between a proximal position
19	corresponding to the proximal position of the cannula and a distal
20	position corresponding to the distal position of the cannula; and
21	carrier drive means, engageable with the first and second
22	carriers, for sequentially driving the first carrier from its first position to
23	its second position and then driving the second carrier from its first
24	position to its second position.
25	
26	16. The biopsy device of Claim 15, wherein the carrier drive means
27	comprises:
28	a motor having a drive shaft;

1	a drive screw coupled for rotation with the drive shaft;
2	a screw-driven mechanism coupled between the drive screw and
3	the carrier, whereby rotation of the drive screw in a first direction
4	moves the carrier from the first position to the second position.
5	
6	17. The biopsy device of Claim 14, wherein the first and second tissue
7	ablation elements are activated by radio frequency electrical current.
8	
9	18. The biopsy device of Claim 15, wherein the stylet is removably
10	mounted in the first carrier and the cannula is removably mounted in the
11	second carrier.
12	
13	19. The biopsy device of Claim 14, wherein the stylet comprises:
14	a shaft having a proximal end and a distal end and defining a
15	longitudinal axis therebetween; and
16	a substantially hemispherical head fixed to the distal end of the
17	shaft, the second tissue ablation element extending distally from the
18	head.
19	
20	20. The biopsy device of Claim 19, wherein the first and second
21	ablation elements are energized by radio frequency electrical current, and
22	wherein the second ablation element comprises an arcuate length of electrical
23	conductor having a radius of curvature that is substantially coplanar with the
24	longitudinal axis of the shaft.
25	
26	21. The biopsy device of Claim 17, wherein the first ablation element
27	is an ablation electrode, and wherein the cannula includes a return electrode
28	spaced from the ablation electrode.

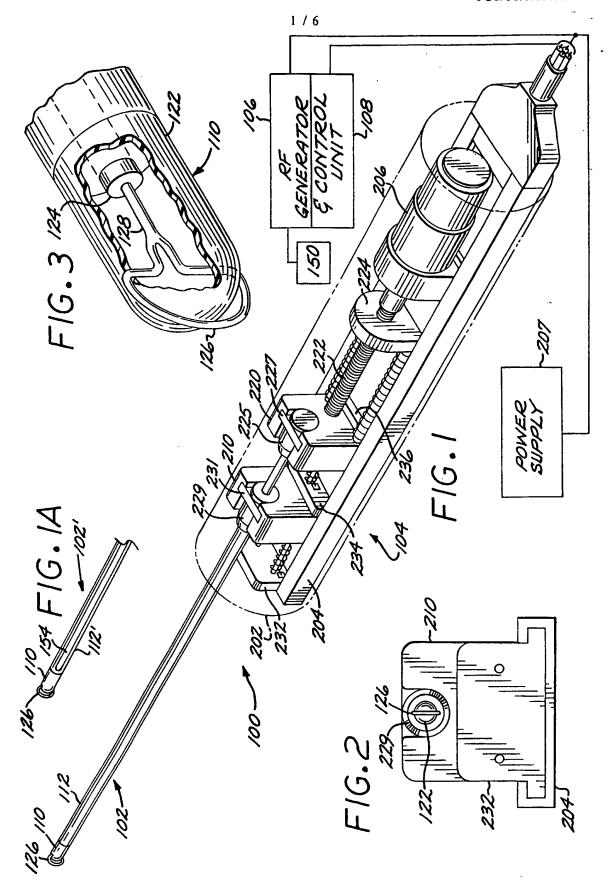
WO 00/16697

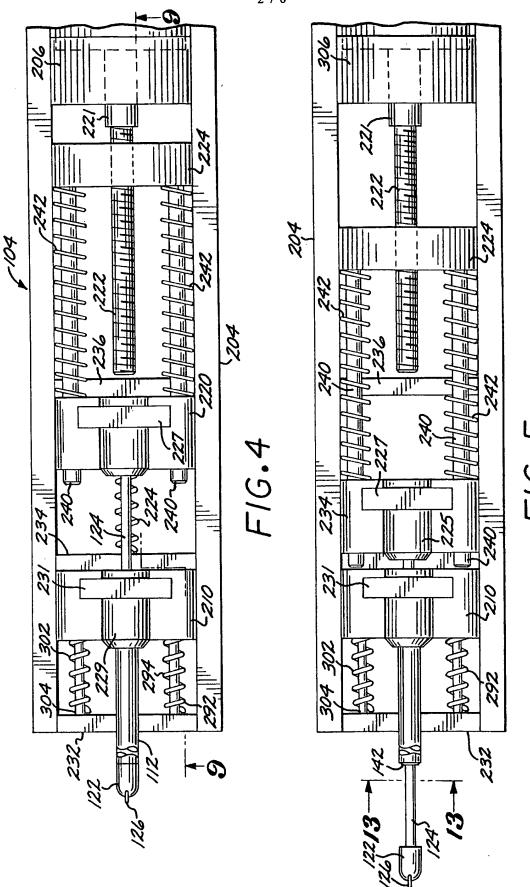
31

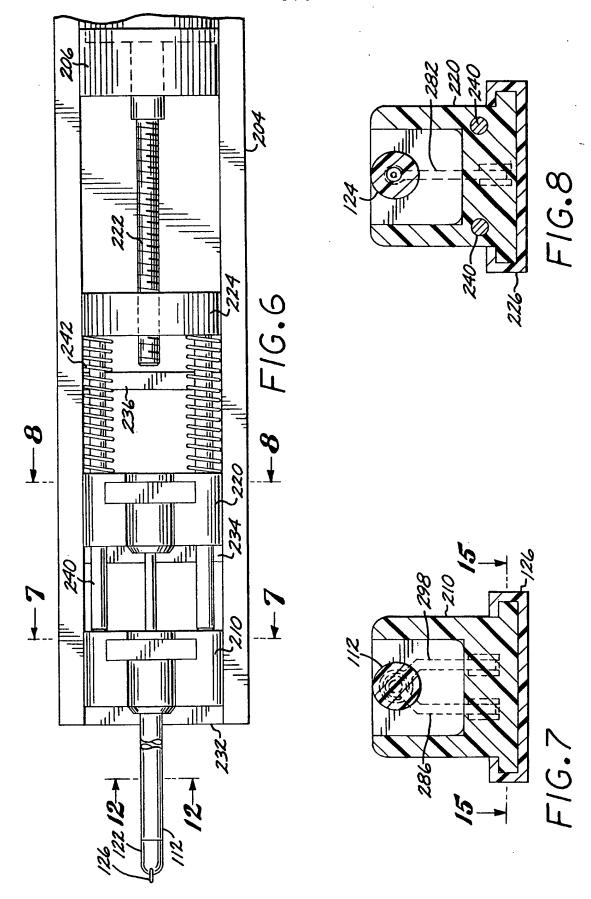
PCT/US99/21416

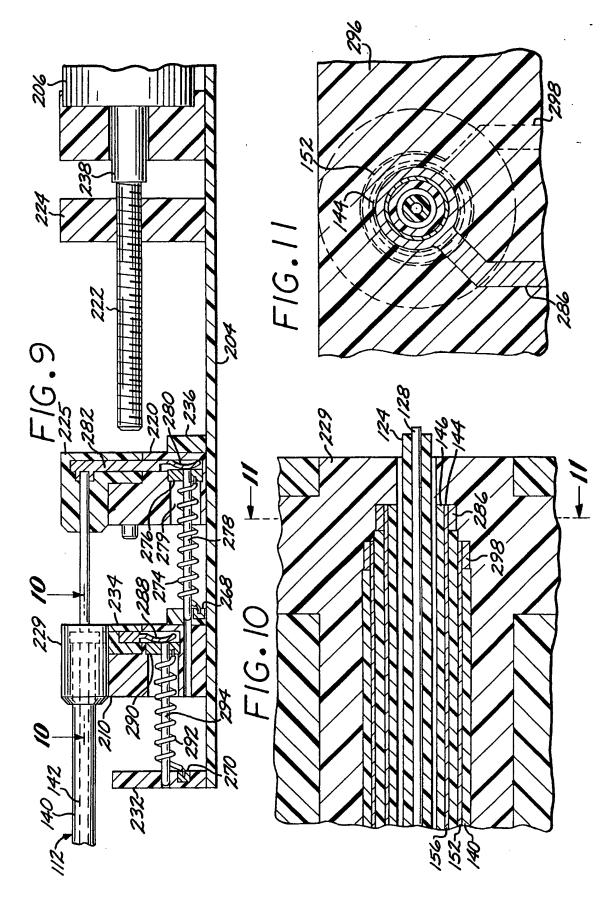
1	22. The biopsy device of Claim 21, wherein the cannula includes an
2	elongate aperture along a portion of its length, and wherein the return
3	electrode comprises a length of conductor contained within the cannula, at
4	least a portion of the conductor being exposed through the elongate aperture.
5	
6	23. A method of taking a tissue sample from a targeted subcutaneous
7	tissue mass within the body of a patient, comprising the steps of:
8	providing a probe comprising a cannula having a distal end with
9	a first tissue ablation element, and a stylet disposed coaxially within the
10	probe for axial movement therein between a withdrawn position and an
11	extended position relative to the distal end of the cannula, the stylet
12	having a distal end with a second tissue ablation element;
13	while activating the second ablation element with energy of a
14	type and quantity that causes tissue ablation, advancing the probe by
15	tissue ablation, with the stylet in the withdrawn position, into the
16	patient's body toward the targeted tissue mass;
17	with the second ablation element activated, moving the stylet to
18	its extended position so that it penetrates the targeted tissue mass by
19	ablation, while creating a gap between the second ablation element and
20	the distal end of the cannula that fills with a portion of the tissue from
21	the targeted tissue mass;
22	while activating the first ablation element with energy of a type
23	and quantity that causes tissue ablation, moving the cannula distally
24	relative to the stylet so as to close the gap, thereby capturing the portion
25	of the tissue mass within the cannula; and
26	withdrawing the probe from the body with the portion of the
27	tissue mass captured within the cannula.

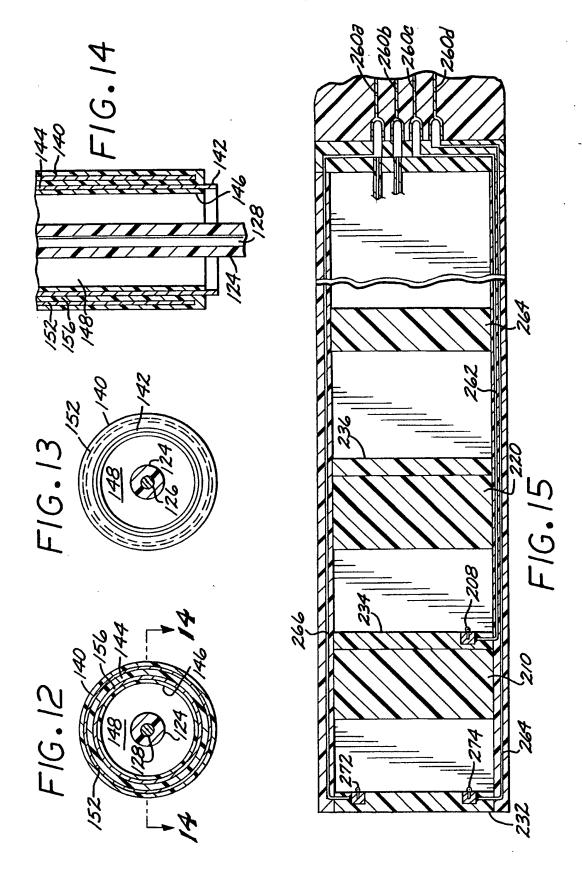
	·
1	24. The method of Claim 23, wherein the first and second ablation
2	elements are activated with radio frequency electrical current.
3	
4	25. The method of Claim 23, wherein the stylet and the cannula are
5	movably mounted on a base, wherein the cannula is movable between a
6	proximal position and a distal position relative to the base, wherein the
7	cannula is in the proximal position during the steps of advancing the probe and
8	of moving the stylet, and wherein the step of moving the cannula includes the
9	step of moving the cannula from its proximal position to its distal position.
10	
11	26. The method of Claim 23, wherein the steps of moving the stylet
12	and moving the cannula are performed by an electrically powered driving
13	mechanism.
14	·
15	27. The method of Claim 23, wherein the step of moving the stylet
16	creates a narrow slice through the targeted tissue mass.











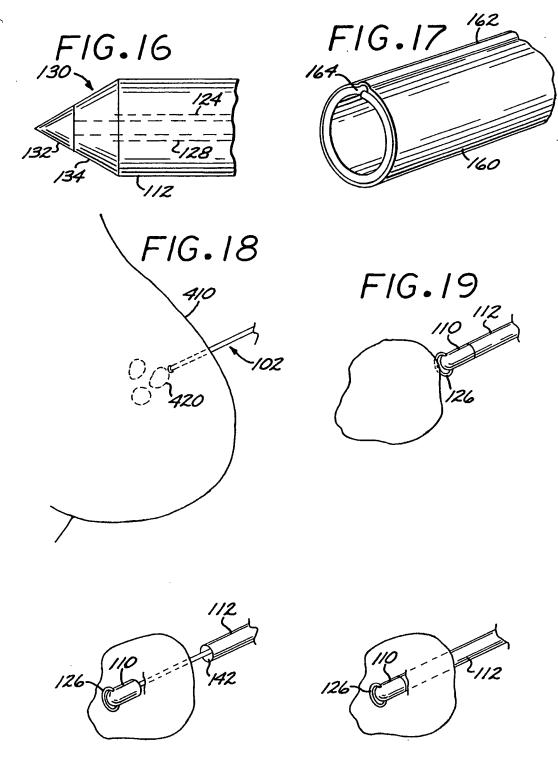


FIG. 20

FIG.21

This Page is Inserted by IFW Indexing and Scanning Operations and is not part of the Official Record

BEST AVAILABLE IMAGES

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images include but are not limited to the items checked:

BLACK BORDERS

IMAGE CUT OFF AT TOP, BOTTOM OR SIDES

FADED TEXT OR DRAWING

BLURRED OR ILLEGIBLE TEXT OR DRAWING

SKEWED/SLANTED IMAGES

COLOR OR BLACK AND WHITE PHOTOGRAPHS

GRAY SCALE DOCUMENTS

LINES OR MARKS ON ORIGINAL DOCUMENT

REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY

IMAGES ARE BEST AVAILABLE COPY.

☐ OTHER:

As rescanning these documents will not correct the image problems checked, please do not report these problems to the IFW Image Problem Mailbox.